The surgical management of spinal deformity has always been a challenging and complex problem. Throughout the 20th century, numerous surgery-related innovations were developed to correct this disorder effectively. Current instrumentation used to treat degenerative and traumatic spinal conditions was largely developed for the management of spinal deformity.

EARLY HISTORY OF PROCEDURES TO CORRECT SPINAL DEFORMITY

Early attempts to correct spinal deformity were largely nonsurgical and involved the use of external braces, traction, and casts. One unsuccessful surgical approach introduced by Jules Guerin in 1839 involved percutaneous vasotomies of the vertebral musculature with postoperative brace therapy.24 Only in the late 19th century did surgeons begin to devise effective methods for correcting the deformed spine internally.

In 1891, Hadra attempted wiring of the spinous processes in a patient with progressive deformity due to Pott disease and successfully stabilized the spinal fracture.9 In 1911 Hibbs introduced the concept of noninstrumentation-induced osseous fusion for stabilization of a deformed spine.13,25 Although this procedure initially provided stabilization, it relied heavily on the use of casts and did not ultimately provide deformity correction.

Until the advent of antibiotic agents to treat tuberculosis and the discovery of a vaccine to eradicate polio, large populations of patients suffered from these disorders. With little or no effective medical therapy, patients with long-standing disease often developed spondylitis and subsequent kyphoscoliosis. In patients with polio, the severe spinal deformities frequently led to cardiopulmonary compromise and death. Patients were placed in various types of braces or contoured plaster casts to halt the progression of the spinal deformity, but these treatments were often ineffective. Prior to the 20th century, it was believed that scoliosis, regardless of origin, was caused by poor posture. Thus, most attempts to resolve this deformity were aimed at correcting posture. Methods included extending the spine through an external axial distraction device, applying vests and casts to mold a correct curvature for the spine, or using braces.14,26

Fritz Lange,17 who treated patients with tuberculous spondylitis in the early 1900s, was one of the first physicians to use foreign materials to supplement and return function to parts of the human body. He thought that parts of the body that had a purely mechanical function could be replaced, including those parts.
involved in movement and support. He hypothesized that since orthopedic surgeons used splints to support long bone fractures, such a method might be successfully applied to correct the deformed or spondylotic spine. External splints for the deformed spine, he found, were inadequate, and he began to perform surgery to splint the spine internally by using an “artificial spinal column of steel.” In this procedure 4-mm-thick steel wires, one on each side of the spinous processes, were placed under the muscles and fastened using silver wires from above and below. This method, however, led to infection and irritation from the wires’ sharp edges. Lange began research in animals to determine an appropriate metal that would reduce these two complications. In 1908, he again tried using steel wires, this time 5-mm thick and 10-cm long, coated with tin, and with tin knobs on either end to reduce irritation; he fastened these to the spinous processes by using paraffin-sublimate silk. Postoperatively, the patient was kept in a plaster-of-paris jacket for as long as 6 weeks and then was slowly mobilized. He found that internal fixation induced faster healing than brace therapy alone. Although he was successful with a small number of patients, the goal of surgical treatment at this time was halting the progression of deformity rather than correcting it.

MODERN ERA OF SPINAL INSTRUMENTATION

Major developments in correcting the deformed spine did not occur until Harrington addressed the problem of the spondylitic spine in patients with poliomyelitis. These patients often suffered from much pain due to the changed curvature of their spine. Poliomyelitis had again achieved epidemic proportions in the 1940s, leaving patients with debilitating spinal deformities. These patients were frequently treated at Jefferson Davis City–County Hospital, where Harrington worked (Fig. 1). Polio-related trunk involvement often led to scoliosis and cardiopulmonary compromise. The placement of inadequate casts or the undertaking of major surgery usually yielded catastrophic results. Harrington initially tried to correct the scoliotic curvature by correcting the position of the facet joints by using screws. The initial results were encouraging, but the long-term results were poor. During this period techniques advanced from the use of facet screws alone, to the placement of hooks on posterior elements, to the use of combinations of hooks and rods made of stainless steel. Harrington hand made the early instrumentation. When the metal instrumentation failed over the long term, he worked with engineers to develop metals that could undergo more repetitive stress. He also decided to use concurrent fusion techniques with bone graft to supplement fixation strength. In this way patients required fewer days of postoperative immobilization. Although initially used to treat patients with polio-related deformity, these procedures were then used to treat idiopathic scoliosis as well. Harrington began teaching his technique at other institutions. As it became more widely used, broader applications followed. Through the efforts of Harrington, Moe alone and with coworkers, the procedure was used to test other causes of spinal deformity, including traumatic fractures, spondylolisthesis, and idiopathic scoliosis. The idea of using internal stabilization to correct a spinal deformity marks the beginning of the modern era of spinal instrumentation.

The Harrington procedure was refined by the 1970s. The new technique consisted of hooks applied to both the cranial and caudal ends of a deformity; the hooks were then attached to rods (Fig. 2). Distraction was used to reduce the deformity. This was then followed by an osseous fusion. This was clearly the first attempt to correct spinal deformity surgically rather than merely provide stabilization. The technique was used successfully to treat hundreds of patients with idiopathic, neuromuscular, and acquired scoliosis. As longer follow-up data became
available, several problems became apparent. In Harrington’s system, because only posterior instrumentation was applied, a long construct without segmental fixation was required. This led occasionally to loosening of the instrumentation, and a reoperation was required to remove the rods after the segments were fused. It often involved fusion down to the sacrum, which led to the loss of lumbar lordosis and flat-back syndrome. These disadvantages provided the impetus for the next wave of changes.

In 1976, Luque instrumentation was introduced for posterior segmental fixation of the spine. This procedure involved multiple points of fixation by using sublaminar wires to create a more biomechanically sound construct. The goal was to reduce the need for external immobilization. Segmental instrumentation involved steel wire loops that were placed under the lamina at various levels and over prebent rods (Fig. 3). Although this technique was an improvement, it still failed to address some of the problems inherent to a long posterior construct. In addition, a significant incidence of neurological complications was demonstrated.27

Correction and stabilization of scoliotic deformity via an anterior approach was also introduced in the 1970s. This was a major advance in the field of spinal deformity surgery. The anterior approach allowed for the placement of shorter constructs and better correction of the deformity. Dwyer, et al.,7 reported using anterior instrumentation. They believed that scoliotic deformities could be approached in two ways, either by stretching the concave side of the curved column or by shortening the long convex side. Titanium screws were inserted into the VB on the convex side. With the aid of plates over these screws, a titanium cable is threaded through the screw heads, and the distance is shortened between the screws by a tensioning device (Fig. 4). By continuing this process down each level of the spine, a bent column would become straighter. Their patients wore a jacket to restrict movement for up to 3 months postoperatively.

The development of Zielke instrumentation resulted in greater correction of deformities than previous techniques.29 This method improved on the Dwyer technique by requiring that the VB screws be placed more posteriorly (Fig. 5) to enhance the derotation effect and reduce the incidence of iatrogenic kyphosis.24 Because anterior techniques do not allow for immobilization and fusion of as many segments as posterior techniques, the incidence of flatback deformity is reduced.

Although excellent correction of deformity was possible via the anterior approach, significant incidences of pseudoarthrosis, hardware failure, and loss of correction with the single rod technique remained.15 In an attempt to overcome these shortcomings, next-generation anterior

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**Fig. 3.** Preoperative (A) and postoperative images (B) obtained in a patient with kyphoscoliosis. Posterior Luque rod instrumentation that was placed in the thoracolumbar spine. From Kostuik, 1992; reprinted with permission from Elsevier Science.

**Fig. 4.** Photographs demonstrating the Dwyer technique for distraction of the spine via an anterior approach. From Dwyer, et al., 1969; reprinted with permission from Lippincott.

**Fig. 5.** Drawings demonstrating the Zielke method for anterior instrumentation and VB screw placement in a scoliotic curve. *Left:* Screw placement from the convex to the concave side. *Center:* Screw placement for a hyperlordotic curve. *Right:* Lateral view of screw placement. From Moe, et al., 1983; reprinted with permission from Lippincott.

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instrumentation, which involves a dual-rod technique, was introduced. The Kaneda system involves the placement of two screws in each VB that are attached to two rods; this system allows for better derotation and creates a biomechanically stronger construct (Fig. 6). Anterior approaches are useful for thoracolumbar curves down to L-5 but cannot be used alone if there is a significant thoracic kyphosis.

The next major advance was the development of transpedicular fixation of the thoracolumbar spine. Biomechanically, pedicle screws are superior to other posterior materials (that is, hooks and sublaminar wires) with respect to pullout strength and load-bearing capacity. They provide three-column fixation of the spine, which can be used to rotate, distract, or compress motion segments prior to fusion. The CD fixation system was introduced in the 1980s. In this system the goal was to combine the rigidity of segmental fixation with curve derotation to obtain correction. All three elements of instrumentation—hooks, rods, and screws—were used. The hardware consists of posterior instrumentation with 7-mm rods, a series of pedicular and laminar hooks that can be secured to the rod at any point along its length and in any transverse axis of rotation, and transverse approximators. The CD allows for distraction, compression, and derotation of the scoliotic deformity. In the initial study of patients with idiopathic scoliosis treated with the CD system, significant reduction of their curvature was achieved.

Further experience with the CD system showed that derotation of the scoliotic spine by rotation of the rod does not always fully correct the deformity. In addition, the spine can become unbalanced above and below the construct. These shortcomings led to the development of a newer generation of pedicle screws and hooks. The USS was designed so that the cranial and caudal ends of the construct are rigidly fixed to two rods to create a frame. The screws are placed in the most caudal and cranial segments of the deformity, and a rod is placed between them to create a frame. Instrumentation is then placed in each intervening vertebral segment, and the VBs are rotated and/or translated into the frame (Fig. 7). Recently, thoracic pedicle screws have been used as an alternative to hooks. They provide better anchor points, and the authors of clinical studies have shown that more effective curve correction can be achieved using these devices than with hooks. The Texas Scottish Rite Hospital instrumentation system involves principles of correction similar to those of the USS but also has side-loading connectors that make revision surgery easier. The latest generation of pedicle screws have polyaxial heads that facilitate rod placement in cases in which the pedicles are not well aligned (Fig. 8).

In the 1990s further developments in the fields of surgical endoscopy led to the application of thoracoscopy to spinal surgery. Video-assisted thoracoscopy has been used to perform anterior release as well as anterior fusion and stabilization in cases of spinal deformity. Morbidity seems to be reduced with this approach. Further studies are necessary to validate the effectiveness of this newer technology.

CONCLUSIONS

Advancements in the field of spinal deformity surgery have improved the quality of life of many patients. Over the course of the 20th century, antibiotic agents reduced the incidence of tuberculosis and vaccines have virtually eliminated polio. The late-stage deformities secondary to these conditions are hardly seen by the present-day spine surgeon. The problems initially addressed by spine surgeons, such as the complexity of kyphoscoliosis, however, remain. The goals of current and future minimally inva-
sive techniques are to achieve the original aims with shorter recovery time.

References


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